

Asian Journal of Pharmaceutical and Health Sciences

www.ajphs.com



Formulation and evaluation of floating tablets of gliclazide employing HPMCK100M, starch acetate and carbopol 934p

K.P.R. Chowdary and S. Areefulla Hussainy **

- 1. University College of Pharmaceutical Sciences, Andhra University, Visakhapatnam -530 003, India.
- 2. MESCO College of Pharmacy, Mustaidpura, Karwan Road, Hyderabad-500 006, India.

ARTICLE HISTORY

Received: 31.10.2011

Accepted: 2.12.2012

Available online: 10.05.2012

Keywords:

Floating tablets, HPMC, Starch acetate, Carbopol.

*Corresponding author:

Email: areefulla581@gmail.com

Mobile: +91 9985356190

ABSTRACT

The objective of the present study is to evaluate HPMC K100M, Starch acetate and Carbopol 934P as matrix formers in this design of floating tablets of gliclazide, a poorly water soluble drug. Floating tablets of gliclazide (60 mg) were formulated employing (i) HPMC K100M (ii) Starch acetate and (iii) Carbopol 934P as matrix formers at 30% and 50% strength, sodium bicarbonate at 7.5%, 10% & 12.5% strength as gas generating agent and bees wax (10%) as floating enhancer and the tablets were evaluated for floating and drug releases characteristics. Gliclazide floating tablets formulated employing HPMC K100M and Starch acetate as matrix formers at 50% strength and containing sodium bicarbonate (12.5%) as gas generating agent exhibited floating over 44 to 48 h with a floating lag time of less than 50sec. These floating tablets also gave slow and controlled release of gliclazide over 24 h and were found suitable for once a day administration (24h). HPMC K100M and Starch acetate were better suitable as matrix formers than Carbopol 934P for floating tablets of gliclazide, a poorly water soluble

INTRODUCTION

The oral route of drug administration is the most convenient and commonly used method of drug delivery. However, this route has certain problems such as unpredictable gastric emptying rate, short gastro-intestinal transit time (8-12 h) and existence of an absorption window in the gastric and upper small intestine for several drugs[1,2] leading to low and variable oral absorption over shorter period of time. The real issue in the development of oral drug delivery systems is to prolong the residence time of the dosage form in the stomach or upper g.i.tract until the drug is completely released and absorbed.

Several approaches are currently used to retain the dosage form in the stomach .These include bioadhesive systems [3] swelling and expanding systems [4,5], floating systems [6,7] and other delayed gastric emptying devices[8,9]. The principle of floating tablets offers a simple and practical approach to achieve increased gastric residence time to enhance the bioavailability and to obtain controlled release. Floating tablets are designed based on gas generating principle. Design of floating tablets needs a strong matrix forming polymer. The objective of the present study is to evaluate HPMC K100M, Starch acetate and Carbopol 934P as matrix formers in the design of floating tablets of gliclazide, a poorly water soluble drug.

Gliclazide is an effective oral antidiabetic agent that belongs to the sulfonyl ureas drug class and is widely prescribed in the management of Non insulin dependent (Type II) diabetes mellitus. It is poorly soluble in aquoes fluids and is majorly absorbed from stomach [10]. Gastro retentive controlled release drug delivery system are needed for gliclazide to enhance its oral bioavailability and also for better control of blood glucose levels to prevent hypoglycaemia to enhance clinical efficiency and patient compliance. Floating tablets of gliclazide were designed in the present study to enhance its bioavailability and to achieve controlled release over 24 h for once a day administration. Floating tablets of gliclazide were designed employing HPMC K100M, Starch acetate and Carbopol 934P as matrix formers, sodium bicarbonate as gas generating agent and bees wax as floating enhancer and the tablets prepared were evaluated for floating and drug release characteristics.

MATERIALS AND METHODS

Gliclazide was a gift sample from M/s. Micro Labs. Ltd., Pondicherry. Hydroxy propyl methyl cellulose K100M, Starch acetate (DS 2.72), Carbopol 934P and Bees wax, I.P were procured from commercial sources. All other materials used were of Pharmacopoeial grade.

Preparation of floating tablets

Matrix tablets each containing 60 mg of gliclazide were formulated employing (i) HPMC K100M (ii) Starch acetate and (iii) Carbopol 934P, each at 30 and 50 % concentration in the formula. Sodium bicarbonate was used as gas generating agent at 7.5%, 10% and 12.5 % strength in each case. Bess wax was used

as floating enhancer at 10% concentration in all the formulations.

The required quantities of gliclazide, HPMC K100M or Starch acetate, sodium bicarbonate, bees wax, lactose were thoroughly mixed in a mortar by following geometric dilution technique. The granulating fluid (a mixture of water and alcohol in 1:1ratio) was added and mixed thoroughly to form a dough mass. The mass was passed through mesh No.12 to obtain wet granules. The wet granules were dried at 600C for 2 h. The dried granules were passed through mesh No. 16 to break the aggregates. The lubricants talc (2%) and magnesium stearate (2%) were passed through mesh No. 60 on to the dry granules and blended in a closed polyethylene bag. The tablet granules were compressed into tablets on a 16-station tablet punching machine (M/s Cadmach Machinaries Pvt. Ltd., Ahmedabad) to a hardness of 7-8.5Kg/cm2. In the case of Carbopol 934P the tablets were prepared by direct compression method.

Evaluation of tablets

Hardness of the tablets was tested using a Monsanto hardness tester. Friability of the tablets was determined in a Roche friabilator. Disintegration time of the tablets was determined using a thermonic tablet disintegration test machine using water, 0.1N HCl and phosphate buffer of pH7.4 as the test fluids.

Estimation of gliclazide

An ultraviolet (UV) spectrophotometric method based on the measurement of absorbance at 229 nm in 0.1N hydrochloric acid was used for the estimation of gliclazide. The method obeyed Beer-Lambert's law in the concentration range of $1-10\mu m/mL$. When a standard drug solution was assayed repeatedly (n=6), the relative error (accuracy) and coefficient of variation (precision) were found to be 0.65% and 1.75%, respectively. No interference from the excipients used was observed.

Floating lag time and floating time

In Vitro buoyancy was determined by measuring floating lag time and duration of floating. The tablets were placed in a 250 ml glass beaker containing 0.1N HCl. The time required for the tablet to rise to the surface and float was determined as floating lag time. The duration in which the tablet remains floating was determined as floating time.

Drug release study

Drug release from the floating tablets was studied using 8-

Table No.1 : Composition and Physical properties of Gliclazide Floating Tablets Formulated Employing Various Polymers

Formulation	Matrix composition	Gliclazide content (mg/tablet)	Hardness (Kg/cm²)	Friability (weight loss%)	Floating lag time (min-sec.)	Floating time (h)
GF1	HPMC K100M (30%), Sod. Bicarb (7.5%)	59.4	7.5	0.4	28.00	20
GF2	HPMC K100M (50%), Sod. Bicarb (7.5%)	60.2	8.0	0.6	27.00	31
GF3	HPMC K100M (30%), Sod. Bicarb (10%)	58.5	7.0	0.5	31.00	36
GF4	HPMC K100M (50%), Sod. Bicarb (10%)	59.8	7.5	0.2	1.20	44
GF5	HPMC K100M (30%), Sod. Bicarb (12.5%)	59.6	7.0	0.4	0.60	44
GF6	HPMC K100M (50%), Sod. Bicarb (12.5%)	61.2	8.0	0.6	0.50	44
GSA1	Starch acetate (30%), Sod. Bicarb (7.5%)	59.8	7.5	0.1	25.00	21
GSA2	Starch acetate (50%), Sod. Bicarb (7.5%)	60.2	7.0	0.6	22.00	30
GSA3	Starch acetate (30%), Sod. Bicarb (10%)	61.5	8.5	0.3	28.00	34
GSA4	Starch acetate (50%), Sod. Bicarb (10%)	60.2	8.5	0.6	0.08	34
GSA5	Starch acetate (30%), Sod. Bicarb (12.5%)	59.8	8.0	0.4	0.24	44
GSA6	Starch acetate (50%), Sod. Bicarb (12.5%)	60.2	8.5	0.2	0.18	48
GC1	Carbopol 934P (30%), Sod. Bicarb (7.5%)	59.2	7.5	0.4	45.00	20
GC2	Carbopol 934P (50%), Sod. Bicarb (7.5%)	60.6	8.5	0.3	40.00	20
GC3	Carbopol 934P (30%), Sod. Bicarb (10%)	59.5	7.0	0.5	36.00	20
GC4	Carbopol 934P (50%), Sod. Bicarb (10%)	60.8	8.0	0.2	42.00	5-6
GC5	Carbopol 934P (30%), Sod. Bicarb (12.5%)	61.6	7.5	0.4	55.00	5-6
GC6	Carbopol 934P (50%), Sod. Bicarb (12.5%)	60.2	8.0	0.6	60.00	4-7

station dissolution rate test apparatus (Labindia, Disso 2000) employing a paddle stirrer at 50 rpm and at a temperature of $37\pm1^{\circ}$ C. Hydrochloric acid, 0.1N (900 mL) was used as dissolution fluid. A 5mL aliquot of dissolution medium was withdrawn through a filter (0.45µm) at different time intervals and assayed spectrophotometrically by measuring absorbance at 229 nm. All drug release experiments were conducted in triplicate(n=3).

Data Analysis

Drug release data were analyzed as per Zero order, first order. Higuichi [11] and Peppas [12] equation models to assess drug release kinetics and mechanism from the tablets.

RESULTS AND DISCUSSION

Matrix tablets of gliclazide were prepared employing (i) HPMC K100M (ii) Starch acetate and (iii) Carbopol 934P as matrix formers, sodium bicarbonate as gas generating agent and bees wax as floating enhancer with an objective of evaluating HPMC K100M, Starch acetate and Carbopol 934P as matrix material for floating tablets of gliclazide, a poorly water soluble drug.

Hardness of the tablets was in the range 7-8.5 Kg/cm2. Weight loss in the friability test was less than 0.6% in all the cases. All the tablets prepared contained gliclazide within $100\pm3\%$ of the labelled claim. All the tablets prepared were found to be non-disintegrating in water and aqueous acidic (pH 1.2) and alkaline (pH7.4) fluids. As such, the prepared tablets were of good quality with regard to drug content, hardness and friability. In the *in vitro* buoyancy study, the floating lag time of various tablets was in the range 8 seconds to 60 minutes.

Formulations GF4, GF5, GF6 and GSA4, GSA5, GSA6 exhibited floating over 34-48 h with a floating lag time of less than 80 seconds. Tablets formulated employing HPMC K100M and Starch acetate at 50% strength and sodium bicarbonate at 12.5% strength (GF6 and GSA6) exhibited good floating characteristics, a floating time of 44 and 48h respectively after a lag time of 18-50sec. Tablets formulated employing Carbopol 934P as matrix former exhibited a floating lag time of 1h and a floating time of 4-7 hours. As such HPMC K100M and Starch acetate are considered as better matrix formers than Carbopol 934P for floating tablets employing sodium bicarbonate (12.5%) as gas generating agent.

Gliclazide release parameters of the floating tablets formulated are summarized in Table-2. Drug release from the prepared tablets was slow, and spread over more than 24h and depended on the polymer used and its strength and concentration of sodium bicarbonate in the tablets. Gliclazide release followed first order kinetics. The correlation coefficient (r^2) values were higher in first order model than those in the zero order model (Table-3) in all the cases. First order release rate constants (K_1) are given in Table-2. When the release data were analysed as per Peppas equation, the release exponent 'n' was found to be in the range 0.517 1.012 indicating 'non-Fickian diffusion' as the release mechanism from all the floating tablets prepared.

Overall, as the polymer concentration was increased, the release rate (K₁) was decreased with all the polymers. When the sodium bicarbonate concentration was increased, the floating time was increased and the release rate was decreased. Tablets formulated employing Carbopol 934P gave rapid release when compared to those formulated with HPMC K100M and Starch

Table No.2: Release Characteristics of Floating Tablets of Gliclazide Formulated Employing Various Polymers

Formulation	T ₅₀	T ₉₀	\mathbf{K}_0	. Kı	'n' in Peppas
	(h)	(h)	(mg/h)	$(h^{-1}) \times 10$	equation
GF1	7	>24	2.948	0.0825	0.616
GF2	9	20	2.896	0.0729	0.517
GF3	10	>24	2,832	0.0712	0.588
GF4	12	>24	2.769	0.0677	0.982
GF5	7	20	3.612	0.1052	0.611
GF6	9	16	4.147	0.1489	0.830
GSA1	10	24	2.842	0.9244	0.787
GSA2	12	>24	2.597	0.8274	1.012
GSA3	10	24	2.842	0.9244	0.787
GSA4	10	24	2.865	0.9610	0.810
GSA5	8	20	3.037	1.1763	0.623
GSA6	5	10	4,246	2.6765	0.623
GC1	7	20	3.963	0.1187	0.725
GC2	4	20	4.873	0.1828	0.929
GC3	5	9	5.098	0.2561	0.609
GC4	5	20	4.912	0.1829	0.873
GC5	8	11	4.318	0.2337	0.564
GC6	4	10	5.07	0.2547	0.642

Table No.3: Correlation coefficient (r²) Values in the Analysis of Release Data as per Various Kinetic Models

<u>-</u>							
Formulation	Zero order	First order	Higuchi	Peppas equation			
GF1	0.9384	0.9796	0.9353	0.9898			
GF2	0.9694	0.9447	0.7425	0.8837			
GF3	0.9821	0.9640	0.7914	0.9322			
GF4	0.9545	0.9807	0.9298	0.9635			
GF5	0.9913	0.9700	0.8227	0.9548			
GF6	0.9645	0.8435	0.7481	0.9665			
GSA1	0.9951	0.9918	0.9850	0.9977			
GSA2	0.9945	0.9694	0.9569	0.9942			
GSA3	0.9951	0.9918	0.9850	0.9977			
GSA4	0.9963	0.9891	0.9806	0.9937			
GSA5	0.9856	0.9929	0.9954	0.9971			
GSA6	0.9755	0.9383	0.9694	0.9834			
GC1	0.9909	0.9556	0.8061	0.9555			
GC2	0.9177	0.9825	0.9428	0.9695			
GC3	0.9527	0.9652	0.8946	0.9704			
GC4	0.9646	0.9775	0.8946	0.9689			
GC5	0.9604	0.7424	0.7475	0.9267			
GC6	0.9066	0.9877	0.9424	0.9719			

acetate. Overall floating tablets formulated with HPMC K100M and Starch acetate at 50% strength gave slow and complete drug release in 24h and were found to be the best floating formulations developed based on *in vitro* buoyancy and drug release characteristics and these tablets were found suitable for 24h i.e., once-a-day administration.

CONCLUSION

Gliclazide floating tablets formulated employing HPMC K100M and Starch acetate as matrix formers at 50% strength and containing sodium bicarbonate (12.5%) as gas generating agent exhibited floating over 44 to 48 h with a floating lag time of less than 50seconds. These floating tablets also gave slow and controlled release of gliclazide over 24 h and were found suitable for once a day administration (24h). HPMC K100M and Starch acetate were better suitable as matrix formers than Carbopol 934P for floating tablets of gliclazide, a poorly water soluble drug.

REFERENCES

- 1. Agyilirah GA, Green M, Ducret R. Evaluation of the gastric retention properties of a cross-linked polymer coated versus those of a non-disintegrating tablets. Int. J. Pharm. 1991; 75: 241-247.
- 2. Hoffman AF, Pressman JH, Code CF. Controlled entry of orally administered drugs: physiological considerations. Drug Dev. Ind. Pharm. 1983; 9: 1077-1085.
- 3. Santus G, Lazzarini G, Bottoni G. An in vitro-in vivo investigation of oral bioadhesive controlled release furosemide formulations. Eur. J. Pharm. Biopharm. 1997; 44:39-52.
- 4. Deshpande AA, Rhodes CT, Shah NH, Malick AW.

Controlled release drug delivery systems for prolonged gastric residence: an overview. Drug Dev. Ind. Pharm. 1996; 22: 531-539.

- 5. Deshpande AA, Shah NH, Rhodes CT, Malick W. Development of a new controlled-release system for gastric retention. Pharm. Res. 1997; 14: 815-819.
- 6. Menon A, Ritschel WA, Sakr A. Development and evaluation of a monolithic floating dosage form for furosemide. J. Pharm. Sci. 1994;83: 239-245.
- 7. Whitehead L, Fell JT, Collett JH, Sharma HL, Smith AM. Floating dosage forms: an in vivo study demonstrating prolonged gastric retention. J. Control. Rel. 1998; 55: 3-12.
- 8. Singh B.N, Kim K.H. Floating drug delivery system: an approach to oral controlled drug delivery via gastric retention. J.Control. Rel. 2000; 63: 235-259.
- 9. Chawla G, Bansal A. A means to address regional variability in intestinal drug absorption. Pharm. Tech. 2003; 27: 50-68.
- 10. Kottke MK, Chuech HR, Rhodes CT. Comparison of disintegrant and binder activity of three corn starch products. Drug Dev.Ind.Pharm. 1992; 18: 2207-2223.
- 11. Higuichi T, Mechanism of sustained action medication: theoretical analysis of rate of release of solid drugs dispersed in solid matrices. J. Pharm. Sci., 1963;52: 1145-1149. Korsmeyer RW, Gurny R, Doelkar E, Buri P, Peppas NA. Mechanism of solute release from porous hydrophilic polymers. Int. J. Pharm. 1983;15: 25-35.